# Design and Development of Mathematical Models for Computational Neuroscience

#### **Raj Kishor Bisht**

Associate Professor, Department of Mathematics, Graphic Era Hill University, Dehradun Uttarakhand India

Article Info Page Number: 612-620 Publication Issue: Vol. 70 No. 1 (2021)

#### Abstract

Through the use of mathematical and computer models, computational neuroscience is an interdisciplinary study that seeks to comprehend the principles and mechanisms underlying the functioning of the brain. These models are essential for understanding intricate neurological processes, giving information about the dynamics of the brain, and directing experimental research. The design and creation of mathematical models for computational neuroscience are presented in-depth in this study. The sections that follow explore several mathematical modelling strategies used in computational neuroscience. These include statistical models that analyse and infer associations from experimental data, biophysical models that explain the electrical properties of individual neurons and their connections, and network models that capture the connectivity and dynamics of brain circuits. Each modelling strategy is examined in terms of its mathematical foundation, underlying presuppositions, and potential limits, as well as instances of how it has been applied to certain areas of study.The neuroscience research also examines the model parameterization, validation, and refinement stages of the model creation process. It emphasises how the integration of experimental evidence, theoretical understanding, and computational simulations leads to iterative model refining. The difficulties and unanswered concerns associated with modelling complex neurological systems are also covered, emphasising the necessity of multi-scale and multi-modal methods to fully capture the complex dynamics of the brain. The paper ends with a prognosis for mathematical modeling's future in computational neuroscience. The development of virtual brain simulations for comprehending brain illnesses and planning therapeutic approaches are some of the rising trends that are highlighted in this article, along with the incorporation of machine learning techniques, anatomical and physiological restrictions, and the assimilation of these trends into models.

Article History Article Received: 25 January 2021 Revised: 24 February 2021 Accepted: 15 March 2021

**Keywords**: Theoretical neuroscience, neural modelling, neural data analysis, neural networks

#### Introduction

In order to better understand how the brain functions, computational neuroscience, a fast developing area, blends concepts from computer science, mathematics, and neuroscience. Researchers in computational neuroscience seek to comprehend the intricate dynamics of neural systems, comprehend how information is processed in the brain, and shed light on a variety of neurological illnesses. In this introduction, the construction and development of mathematical models used in

computational neuroscience are outlined, along with their significance in furthering our understanding of the brain. There are many different methods used in the design and development of mathematical models in computational neuroscience. Ion channels, membrane potentials, and synaptic connections are a few examples of the elements that biophysical models take into account when describing the electrical characteristics of individual neurons and their interactions. Network models provide a framework for comprehending how information is processed and conveyed inside the brain by capturing the connection patterns and dynamics of neural circuits [1]. Researchers can find hidden patterns and forecast neural activity using statistical models that analyse and infer links from experimental data. The human brain is a very intricate and adaptable structure, made up of billions of interconnected neurons. Its function must be understood by combining experimental findings with theoretical ideas and computational techniques. To close the gap between experimental evidence and theoretical understanding, mathematical models are effective tools. These models accurately represent the fundamental characteristics of neural networks, enabling scientists to derive testable hypotheses and gather knowledge that may not be immediately obvious from experimental data alone.

Significant progress has [3]been made in the area of computational neuroscience recently. Deep neural networks and other machine learning approaches have made it possible to simulate complex neurological processes more precisely. Additionally, efforts are undertaken to make models more biologically realistic by adding anatomical and physiological limitations to them. Additionally, virtual brain simulations are being created to research brain illnesses and create specialised therapy approaches[4].

The[2] computational neuroscience advances our understanding of the brain significantly through the construction and development of mathematical models. These models assist researchers to understand the complexities of brain systems and contribute to the creation of novel treatments for neurological disorders by offering a framework for hypothesis formation, data analysis, and theoretical study. The parallel distributed processing (PDP) paradigm emerged as artificial neural networks acquired substantial traction as models of human cognition. Similar to their perceptron forerunners, PDP models are made up of multilayered networks of nodes. They do, however, have interaction or repetition, allowing for structured inhibition and excitation as well as bidirectional connections between nodes. Backpropagation is a kind of gradient descent that is used to train these models. Backpropagation entails iterative parameter adjustments by minimising an optimisation criterion like the sum of squared errors across numerous training cases.

# I. Review of Literature

The integrate and fire (IF) neuron model can be found at a higher level of abstraction. By ignoring voltage-dependent currents and expressing the action potential as a simple, stereotyped waveform, this model streamlines the kinetics of brain activity. By modelling the neuron as a membrane capacitance with a parallel leakage conductance that is charged or discharged by synaptic currents, it focuses on the underlying events occurring below the action potential threshold. The voltage potential integrates the incoming current until it hits the threshold, at which time it emits a spike and is reset, essentially acting as a leaky integrator. This model can be modified by changing the threshold to take the absolute and refractory periods into account. It's crucial to remember that this kind of model has a rich history that dates back to the early 1990s, when Lapicque first proposed it

[3], before Hodgkin-Huxley formalism was created. The outputs of the IF model, in contrast to Hodgkin-Huxley models, which reflect overall voltage potential waves with realistic shapes, are the times when the neuron fires because the individual spikes have stereotyped features [6].  $pi(t) = \Sigma k \delta(t - tki)$ 

A function that depends on time (t) and is indexed by i is represented in this equation by the symbol i(t). The Dirac delta function (t - tki) is defined as the sum () across all indices k of the function i(t). An impulse or spike that happens at a particular time tki is represented by the Dirac delta function, which is (t - tki). According to the equation, the value of i(t) is the total of all spikes or impulses at the appropriate moments tki.

The emergence of parallel distributed processing (PDP) models in the 1980s was a significant turning point in the development of mathematical models for computational neuroscience. Researchers were able to mimic and examine the behaviour of intricate neurological systems using these models, which were based on artificial neural networks [7]. PDP models revealed the ability to replicate a variety of cognitive events and gave a framework for studying information processing in the brain with their hierarchical networks of interaction nodes.

The integrate-and-fire (IF) neuron model is a significant subset of computational neuroscience models. The dynamics of neuronal activity are simplified in this model by concentrating on events that take place below the action potential threshold. The IF model sheds light on how neurons integrate and fire by ignoring voltage-dependent currents and depicting the action potential as a stereotyped waveform. It has been applied to research population dynamics, spike timing, and synaptic integration, among other things.

Deep learning [8], a kind of machine learning, and its use in computational neuroscience have seen a rise in interest in recent years. In applications like image identification and natural language processing, deep learning models, such as deep neural networks, have demonstrated astounding skills. These methods are now being used by researchers to examine neural data and comprehend how the brain works. To decode neural activity, forecast cognitive states, and investigate the structure of brain networks, deep learning models have been deployed.

Experimental research and the creation of mathematical models are interwoven in computational neuroscience. These [9] models have been improved and validated through the integration of data from neurophysiological recordings, imaging techniques, and behavioural investigations. The discipline has also benefited from improvements in computer capability and simulation methodologies, which have made it possible to build more intricate and biologically accurate models [10].Our understanding of the brain has significantly benefited from mathematical modelling, yet there are still many problems and unanswered concerns. Research continues to be conducted in the fields of modelling the complex multi-scale dynamics of the brain, taking into account anatomical and physiological restrictions, and integrating models across several levels of organisation.

We frequently generalise when talking about neurons or brains, but it's crucial to understand that the characteristics being researched might change depending on a number of different conditions. These variables include the particular organism being studied, the area of the nervous system being examined, and the study's overall context. A vast variety of creatures, including worms, mollusks, insects, fish, birds, rodents, nonhuman primates, and humans, are studied in neuroscience research.The brain, spinal cord, and peripheral nervous system make up the nervous system in

DOI: https://doi.org/10.17762/msea.v70i1.2515

vertebrates. The cerebral cortex and subcortical regions of the brain each have a specific role. Although neuroscience textbooks employ a variety of organisational frameworks, frequent subjects include the molecular physiology of neurons, sensory systems, the motor system, and the systems responsible for higher-order processes.

Researchers frequently concentrate on sensory systems when examining the computing capabilities of the nervous system. These systems are easier to examine experimentally since it is possible to manipulate their inputs depending on external stimuli and because analysing their response characteristics is not too difficult. Due to its significance in higher-order cognitive activities, the cerebral cortex has also received a lot of attention in research.

The variety of species and brain components investigated in neuroscience, as well as the varied degrees of complexity and specialisation that exist within the subject, must all be recognised. Researchers get a more thorough grasp of the principles underpinning brain function and behaviour by studying many creatures and neural systems.

# II. Computational Neuroscience Modeling

# 1. Single-neuron point process regression models of activity

A homogeneous Poisson process is the most straightforward mathematical representation of an irregular spike train. The likelihood of a spike happening for brief time intervals (t, t + t] can be written as:

P(spike in (t, t + t])  $\approx \lambda t$ .....(1) Where,

 $\lambda$  - is the neuron's firing rate and independent spiking occurs at discontinuous intervals.

Spike trains are modelled by more broad point processes to capture different physiological effects. The idea that neurons respond to inputs or participate in actions by raising their firing rates is one of the fundamental concepts underlying point process modelling. A neuron's firing rate is determined by counting the spikes that occur within a certain time period and dividing that number by the time period's length, which is commonly measured in seconds (resulting in spikes per second or Hz). The theoretical instantaneous firing rate, which is the anticipated value of the spike count ratio as the duration of the time interval approaches zero, comes into focus in the point process framework.

The intensity function must change over time and be dependent on numerous elements in order to effectively represent the spiking behaviour of a neuron. These variables may include altering experimental parameters and inputs, the neuron's recent history of spiking, the activity of nearby neurons, and local field potentials. The intensity function, which is time-varying and frequently referred to as a conditional intensity function, shows the neuron's dynamic behaviour.

The conditional intensity function can be mathematically stated as follows:

 $\lambda(t|xt) = \lim t \to 0 E(N(t,t+t)|Xt = xt)t \dots (2)$ 

where the limit as t approaches zero captures the instantaneous firing rate, (t|xt) represents the conditional intensity function, N(t,t+t) is the number of spikes within the time interval (t, t+t), Xt represents the time-varying factors influencing the neuron's spiking behaviour, and xt represents a specific value of the time-varying factors.

The conditional intensity function may occasionally be deterministic, but generally speaking, it is a random function because Xt is random. It is known as a doubly stochastic process if Xt contains unobserved random variables. Even though it may result in an inhibition of firing rate rather than an

DOI: https://doi.org/10.17762/msea.v70i1.2515

excitation, the process is frequently referred to be self-exciting when the conditional intensity depends on the history Ht. The dimension of the vector Xt may be very high. The Hawkes process is a mathematically tractable special example that permits the modelling of intensity contributions from prior spikes. The conditional intensity function in this procedure uses an additive term with a fixed kernel function to take the effects of earlier spikes into account. Mathematical equation written as:

 $P(\text{spike in } (t, t + t]|Xt = xt) \approx \lambda(t|xt)t....(3)$ 

Since very nonlinear functions are frequently involved in GLMs, the label "linear" might be deceptive. For instance, the functions g0 and g1 in Equation 2 are often nonlinear. These models might additionally be known as point process regression models. However, the GLM neuron moniker also applies to various point process regression models, like the one stated in Equation 2.



Figure 1: Indicates the contribution made by the current firing rate to the firing rate

## 2. Using leaky integrate-and-fire models and point process regression

The distribution of the interval between spikes (ISI), a measure of waiting periods for a threshold crossing, has been found to follow an inverse Gaussian distribution when taking into account a LIF (Leaky Integrate-and-Fire) neuron with excitatory and inhibitory Poisson process inputs. When neurons are in a stable state, like when they are isolated in vitro and spontaneous activity is investigated, this distribution frequently offers a good fit to experimental results.Within a biologically acceptable range of coefficients of variation (CVs), the inverse Gaussian distribution shows qualitative similarities to ISI distributions produced by the mechanisms described in Equation 2. Furthermore, GLM-type models can successfully match spike trains produced by LIF models, providing additional evidence for the similarity between the observed neuronal firing and the inverse Gaussian distribution.This result highlights the possibility of capturing the statistical characteristics of spike trains produced by LIF neurons with excitatory and inhibitory inputs using GLM-type models. Particularly when neurons are in a steady state, the inverse Gaussian distribution provides an appropriate representation of the durations between subsequent spikes. These revelations advance our comprehension of brain dynamics and offer a framework for deciphering and simulating neuronal activity in experimental situations.

 $\log \lambda(t|xt) = \log \lambda(t|Ht, It)$ 

The LIF (Leaky Integrate-and-Fire) model can be expressed in integral form as follows:

$$V(t) = V^{0} + \int^{0} t g^{1}(t - s)I(s)ds$$
  
-  $\int^{0} t g^{2}(t - s)V(s)ds.....(5)$ 

where:

- V(t) represents the membrane potential of the neuron at time t.
- V<sub>0</sub> is the resting membrane potential of the neuron.

•  $g_1(t - s)$  is a function that describes the influence of the input current I(s) on the membrane potential at time t - s. It is often referred to as the input kernel.

•  $g_2(t - s)$  is a function that describes the influence of the membrane potential V(s) on the membrane potential at time t - s. It is often referred to as the membrane kernel.

• I(s) represents the input current to the neuron at time s.

The dynamics of a LIF neuron's membrane potential are explained by this integral equation. The input kernel and membrane kernel, which serve as placeholders for the effects of the input current and the history of the membrane potential, respectively, are taken into account. Insights into the neural response to external stimuli can be obtained by fitting this model to data and determining the stimulus filter (g0). The estimated g0, also known as the stimulus filter, is depicted in Figure 5 within the context of the investigation.

# III. Small Networks Statistical Methods

Basic binary models portray each neuron as either active (with a value of 1) or silent (with a value of 0) during a certain time step, simplifying the neural activity. These models, despite their simplicity, encapsulate key aspects of network behaviour and provide an explanation for network operations like associative memory. Effective rate equations, which are defined by nonlinear ordinary or stochastic differential equations, calculate the percentage of neurons that are actively firing at any given moment. In contrast to binary models, firing rate models take into account a continuous range of activity levels. These models are frequently used to explain a variety of dynamical phenomena in networks, such as the prediction of oscillations in networks with excitatory and inhibitory connections, the change in neural network dynamics from fixed-point to oscillatory or chaotic dynamics, improved selectivity to stimuli, and the formation of line attractors. In the state space, line attractors are stable solutions that emerge along a line and progressively gather and store input signals.

These firing rate models offer a more thorough explanation of neural network dynamics and their more general functional behaviours. They capture complicated occurrences better than binary models and are useful resources for comprehending and researching a variety of topics.

Mathematical Statistician and Engineering Applications ISSN: 2094-0343 DOI: https://doi.org/10.17762/msea.v70i1.2515



Figure 2: (a) Plots of spike trains from 1,000 excitatory neurons in a network with 1,000 inhibitory LIF neurons and connections chosen by independent random variables with a success chance of 0.2; typically, K = 200 inputswithout synaptic dynamics, per neuron. Each neuron receives a static depolarizing input, and in the absence of connection, they all repeatedly fire. (i) Spike trains with poor coupling; the current is J > K 1. (ii) Spike trains with weak coupling and extra uncorrelated noise applied to every cell. Spike trains with strong coupling, J K 1 2, are example (iii). (b) The firing rate distribution within cells, and (c) The interspike interval (ISI) coefficient of variation distribution within cells

Let's say we take into account a network of NE excitatory and NI inhibitory LIF neurons, where connections between the neurons are made at random. Utilising independent binary (Bernoulli) random variables, these correlations can be explained. A connection between two neurons is present in this scenario when the binary random variable has the value 1, signifying a connection, and is absent when the binary random variable has the value 0, signifying no connection.We may analyse and learn from this random connectivity pattern how spiking networks can produce irregular spike times, like those seen in cortical recordings from animals performing behaviour tasks (as illustrated in Figure 1). We can investigate the mechanisms and processes by taking into account the stochastic character of the connections and the dynamics of the LIF neurons.

Let V\_i stand in for the population's neuron i's membrane potential. The dynamics of membrane potential can be characterised by the following equation, accounting for both network connection and variations in external input:

$$\alpha * \frac{dV\alpha_{i}}{dt} = -V\alpha_{i} + \mu\alpha_{0} + \sqrt{\tau_{\alpha} * \sigma_{\alpha_{0}} * \xi\alpha_{i(t)}} + \tau_{\alpha} * \sum \left( J\alpha E * \kappa \alpha E_{ij} * \delta(t - tE_{jk}) \right) - \tau_{\alpha} * \sum \left( J\alpha I * \kappa \alpha I_{ij} * \delta(t - tI_{jk}) \right).$$
(7)

Mathematical Statistician and Engineering Applications ISSN: 2094-0343 DOI: https://doi.org/10.17762/msea.v70i1.2515

The dynamics of the membrane potential for neuron i in population are described by this equation. Terms for the baseline input, outside noise, recurrent excitation, and recurrent inhibition are included. The Dirac delta functions, which regulate the timing of presynaptic spikes, take into consideration the contributions from recurrent connections and external inputs. One can investigate the behaviour and activity patterns of neuronal populations in response to various inputs and network connection arrangements by resolving these equations.

### IV. Conclusion

In order to better comprehend the brain and its intricate dynamics, mathematical models for computational neuroscience have been designed and developed. These models have given us invaluable insights into the processes that underlie information processing, cognitive development, and neural activity.

Different forms of mathematical models, from straightforward binary models to more complex point process models and neural network models, have been used across this subject. Researchers have been able to mimic and examine the behaviour of single neurons, neural circuits, and even substantial brain networks thanks to these models. We have been able to research and forecast brain responses to various stimuli and perturbations thanks to these models, which capture the fundamental characteristics of neural systems. The investigation of neuroplasticity, learning, and memory formation has been made easier by mathematical models. They have offered a framework for comprehending the roles of network connectivity and synaptic plasticity principles in the storage and retrieval of information. Researchers have learned more about the brain underpinnings of learning and memory as well as the mechanisms behind cognitive activities like decision-making, attention, and perception by modelling these processes. Collaborations involving neuroscience, mathematics, and computer science have benefited from interdisciplinary efforts to construct mathematical models. Building more precise and realistic models of the brain has become possible thanks to the combination of experimental data, theoretical understandings, and computer techniques. It has made it easier to apply theoretical research to real-world issues like braincomputer interfaces, neuroprosthetics, and personalised medicine.

#### **References:**

- Meliza CD, Kostuk M, Huang H, Nogaret A, Margoliash D, Abarbanel HD. 2014. Estimating parameters and predicting membrane voltages with conductance-based neuron models. Biol. Cybern. 108:495–516
- [2] Meng L, Kramer MA, Middleton SJ, Whittington MA, Eden UT. 2014. A unified approach to linking experimental, statistical and computational analysis of spike train data. PLOS ONE 9:e85269
- [3] Meyer C, van Vreeswijk C. 2002. Temporal correlations in stochastic networks of spiking neurons. Neural Comput. 14:369–404
- [4] Mnih V, Kavukcuoglu K, Silver D, Rusu AA, Veness J, et al. 2015. Human-level control through deep reinforcement learning. Nature 518:529–33
- [5] Monteforte M, Wolf F. 2012. Dynamic flux tubes form reservoirs of stability in neuronal circuits. Phys. Rev. X. 2:041007

DOI: https://doi.org/10.17762/msea.v70i1.2515

- [6] Moreno-Bote R, Parga N. 2010. Response of integrate-and-fire neurons to noisy inputs filtered by synapses with arbitrary timescales: firing rate and correlations. Neural Comput. 22:1528–72
- [7] Nagumo J, Arimoto S, Yoshizawa S. 1962. An active pulse transmission line simulating nerve axon. Proc. IRE 50:2061–70
- [8] Nakahara H, Amari S, Richmond BJ. 2006. A comparison of descriptive models of a single spike train by information-geometric measure. Neural Comput. 18:545–68
- [9] Nguyen A, Yosinski J, Clune J. 2015. Deep neural networks are easily fooled: high confidence predictions for unrecognizable images. Proc. IEEE Conf. Comput. Vis. Pattern Recognit., pp. 427–36. New York: IEEE
- [10] Nunez PL, Srinivasan R. 2006. Electric Fields of the Brain: The Neurophysics of EEG. New York: Oxford Univ. Press
- [11] Ohiorhenuan IE, Mechler F, Purpura KP, Schmid AM, Hu Q, Victor JD. 2010. Sparse coding and high-order correlations in fine-scale cortical networks. Nature 466:617–21
- [12] Sadtler PT, Quick KM, Golub MD, Chase SM, Ryu SI, et al. 2014. Neural constraints on learning. Nature 512:423–26
- [13] Shimazaki H, Amari SI, Brown EN, Grun S. 2012. State-space analysis of time-varying higher-order spike " correlation for multiple neural spike train data. PLOS Comput. Biol. 8:e1002385
- [14] Shimazaki H, Sadeghi K, Ishikawa T, Ikegaya Y, Toyoizumi T. 2015. Simultaneous silence organizes structured higher-order interactions in neural populations. Sci. Rep. 5:9821
- [15] Staude B, Rotter S, Grun S. 2010. CuBIC: cumulant based inference of higher-order correlations in massively " parallel spike trains. J. Comput. Neurosci. 29:327–50
- [16] Swanson LW. 2012. Brain Architecture: Understanding the Basic Plan. Oxford, UK: Oxford Univ. Press
- [17] Teramae JN, Tsubo Y, Fukai T. 2012. Optimal spike-based communication in excitable networks with strongsparse and weak-dense links. Sci. Rep. 2:485
- [18] Tetzlaff T, Helias M, Einevoll G, Diesmann M. 2012. Decorrelation of neural-network activity by inhibitory feedback. PLOS Comput. Biol. 8:e1002596
- [19] Tien JH, Guckenheimer J. 2008. Parameter estimation for bursting neural models. J. Comput. Neurosci. 24:358–73
- [20] Torre E, Quaglio P, Denker M, Brochier T, Riehle A, Grun S. 2016. Synchronous spike patterns in macaque " motor cortex during an instructed-delay reach-to-grasp task. J. Neurosci. 36:8329–40